

FORM PTO-1390
REV. 5-93

US DEPARTMENT OF COMMERCE
PATENT AND TRADEMARK OFFICE

ATTORNEYS DOCKET NUMBER
P01,0178

**TRANSMITTAL LETTER TO THE UNITED STATES
DESIGNATED/ELECTED OFFICE (DO/EO/US)
CONCERNING A FILING UNDER 35 U.S.C. 371**

U.S. APPLICATION NO. (if known, see 37 CFR 1.5).

09/830239

INTERNATIONAL APPLICATION NO.
PCT/SE99/01893

INTERNATIONAL FILING DATE
21 October 1999

PRIORITY DATE CLAIMED
27 October 1998

TITLE OF INVENTION

A HOUSING, WITH A TUBULAR CONNECTOR, FOR A FOR A HEART STIMULATOR

APPLICANT(S) FOR DO/EO/US

PAUL BRAND and ROLF HILL

Applicant herewith submits to the United States Designated/Elected Office (DO/EO/US) the following items and other information:

1. ☒ This is a **FIRST** submission of items concerning a filing under 35 U.S.C. 371.
2. ☐ This is a **SECOND** or **SUBSEQUENT** submission of items concerning a filing under 35 U.S.C. 371.
3. ☒ This express request to begin national examination procedures (35 U.S.C. 371(f)) at any time rather than delay.
4. ☒ A proper Demand for International Preliminary Examination was made by the 19th month from the earliest claimed priority date.
5. ☒ A copy of International Application as filed (35 U.S.C. 371(c)(2)) - drawings attached.
 - a. ☒ is transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ has been transmitted by the International Bureau.
 - c. ☐ is not required, as the application was filed in the United States Receiving Office (RO/US)
6. ☐ A translation of the International Application into English (35 U.S.C. 371(c)(2)) -
7. ☐ Amendments to the claims of the International Application under PCT Article 19 (35 U.S.C. §371(c)(3))
 - a. ☐ are transmitted herewith (required only if not transmitted by the International Bureau).
 - b. ☐ have been transmitted by the International Bureau.
 - c. ☐ have not been made; however, the time limit for making such amendments has NOT expired.
 - d. ☐ have not been made and will not be made.
8. ☐ A translation of the amendments to the claims under PCT Article 19 (35 U.S.C. 371(c)(3)).
9. ☐ An oath or declaration of the inventor(s) (35 U.S.C. 371(c)(4)).
10. ☐ A translation of the annexes to the International Preliminary Examination Report under PCT Article 36 (35 U.S.C. 371(c)(5)).

Items 11. to 16. below concern other document(s) or information included:

11. ☒ An Information Disclosure Statement under 37 C.F.R. 1.97 and 1.98; (PTO 1449, Prior Art, Search Report).
12. ☐ An assignment document for recording. A separate cover sheet in compliance with 37 C.F.R. 3.28 and 3.31 is included. (Separate envelope)
13. ☐ A FIRST preliminary amendment.
 - ☐ A SECOND or SUBSEQUENT preliminary amendment.
14. ☐ A substitute specification, including red-lined version
15. ☐ A change of power of attorney and/or address letter.
16. ☒ Other items or information:
 - a. ☒ Submission of drawings
 - b. ☐ Request for Approval of Drawing Changes
 - c. ☒ Express Mail Label EJ 077704765US

U.S. APPLICATION NO. (if known, see 37 C.F.R. 1.5)

09/830239

INTERNATIONAL APPLICATION NO.
PCT/SE99/01893ATTORNEY'S DOCKET NUMBER
P01,017817. ☒ The following fees are submitted:**BASIC NATIONAL FEE (37 C.F.R. 1.492(a)(1)-(5):**

Search Report has been prepared by the EPO or JPO \$860.00

International preliminary examination fee paid to USPTO (37 C.F.R. 1.482) \$690.00

No international preliminary examination fee paid to USPTO (37 C.F.R. 1.482) but
international search fee paid to USPTO (37 C.F.R. 1.445(a)(2)) \$760.00Neither international preliminary examination fee (37 C.F.R. 1.482) nor international
search fee (37 C.F.R. 1.445(a)(2)) paid to USPTO \$1000.00International preliminary examination fee paid to USPTO (37 C.F.R. 1.482) and all
claims satisfied provisions of PCT Article 33(2)-(4) \$100.00**ENTER APPROPRIATE BASIC FEE AMOUNT =**

CALCULATIONS

PTO USE ONLY

\$ 1000.00

Surcharge of \$130.00 for furnishing the oath or declaration later than ☐ 20 ☐ 30 months from
the earliest claimed priority date (37 C.F.R. 1.492(e)).

\$

Claims

Number Filed

Number Extra

Rate

Total Claims

23

- 20 =

3

X \$18.00

\$

Independent Claims

2

- 3 =

X \$ 80.00

\$

Multiple Dependent Claims

\$270.00 +

\$270.00

TOTAL OF ABOVE CALCULATIONS =

\$1270.00

Reduction by 1/2 for filing by small entity, if applicable. Verified Small Entity statement must
also be filed. (Note 37 C.F.R. 1.9, 1.27, 1.28)

\$

SUBTOTAL =

\$1270.00

Processing fee of \$130.00 for furnishing the English translation later than ☐ 20 ☐ 30 months
from the earliest claimed priority date (37 CFR 1.492(f)).

\$

TOTAL NATIONAL FEE =

1270.00

Fee for recording the enclosed assignment (37 C.F.R. 1.21(h). The assignment must be
accompanied by an appropriate cover sheet (37 C.F.R. 3.28, 3.31). \$40.00 per property +**TOTAL FEES ENCLOSED =**

\$1270.00

Amount to be
refunded

\$

charged

\$

a. ☒ A check in the amount of \$1270.00 to cover the above fees is enclosed.b. ☐ Please charge my Deposit Account No. _____ in the amount of \$ _____ to cover the above fees. A duplicate copy of this
sheet is enclosed.c. ☒ The Commissioner is hereby authorized to charge any additional fees which may be required, or credit any overpayment to Deposit
Account No. **501519**. A duplicate copy of this sheet is enclosed.**NOTE:** Where an appropriate time limit under 37 C.F.R. 1.494 or 1.495 has not been met, a petition to revive (37 C.F.R. 1.137(a) or (b)) must
be filed and granted to restore the application to pending status.**SEND ALL CORRESPONDENCE TO:**Schiff Hardin & Waite
Patent Department
6600 Sears Tower
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SIGNATURE

Steven H. Noll

NAME

28,982 (Registration No.)



-1-

IN THE UNITED STATES DESIGNATED OFFICE
OF THE UNITED STATES PATENT AND TRADEMARK OFFICE
UNDER THE PATENT COOPERATION TREATY-CHAPTER II
AMENDMENT "A" PRIOR TO ACTION AND SUBMISSION OF

5

SUBSTITUTE SPECIFICATION

APPLICANTS: Brand et al.
SERIAL NO.: 09/830,239
FILED: April 24, 2001
TITLE: "A HOUSING, WITH A TUBULAR CONNECTOR, FOR
10 A HEART STIMULATOR"

Assistant Commissioner for Patents,
Washington, D.C. 20231

S I R:

Applicants herewith amend the above-referenced PCT application as
15 follows, and request entry of the Amendment prior to examination in the
United States National Examination Phase.

IN THE SPECIFICATION

Please enter the substitute specification submitted herewith pursuant
to 37 C.F.R. §1.125(b). A marked-up version showing all changes is also
20 submitted herewith. No new matter is added in the substitute specification.

IN THE CLAIMS

On page 13, in line 1, cancel "CLAIMS" and substitute
--**WE CLAIM AS OUR INVENTION:**-- therefor.

Please cancel claims 1-9 and substitute the following claims therefor:
25 10. A pacemaker housing comprising:
a metallic housing enclosure;

5 a connector arrangement adapted to receive a contact plug of an electrode lead, said connector arrangement comprising a tubular member disposed inside said housing and having a first end and a second end opposite said first end, said first end of said tubular member being attached, by an attachment selected from the group consisting of a weld and bond, to an opening in a wall of said housing, and said second end of said tubular member being closed;

10 said tubular member being formed by a tube comprised of a metal attachable to said metal housing by said attachment, said tube having a length and being structurally intact along an entirety of said length;

a plurality of interior elements adapted for mechanical and electrical contact with said contact plug; and

15 an insulating plug disposed in an interior of said tube and having said interior elements mounted therein, said insulating plug being coaxial with said tube and holding said interior elements at respective positions for producing said mechanical and electrical contact with said contact plug.

20 11. A pacer housing as claimed in claim 10 wherein said insulating plug closes said second end of said tubular member with said insulating plug fitting into said tube, and wherein said plug is comprised of ceramic material and is attached to said tube by an attachment technique selected from the group consisting of soldering and bonding.

25 12. A pacer housing as claimed in claim 11 wherein said housing enclosure has a housing interior, and further comprising a metallic tubular

sleeve embedded in said ceramic plug and having an end projecting from said ceramic plug exposing an exterior contact surface for providing electrical contact with said housing interior, and said sleeve having an opposite end which is exposed in an interior of said tubular member to produce an inner contact surface adapted for electrical and mechanical contact with said contact plug.

13. A pacemaker housing as claimed in claim 11 wherein said housing enclosure has an interior, and further comprising a metallic plug embedded in said ceramic plug, said metallic plug having an outer end projecting from said ceramic plug to provide an exterior contact surface for electrical contact with said interior of said housing.

14. A pacemaker housing as claimed in claim 13 wherein said metallic plug has an opposite end with a bore therein in communication with an interior of said ceramic plug, and adapted to receive and electrically contact said contact plug.

15. A pacemaker housing as claimed in claim 11 wherein said housing enclosure has an interior, and wherein said ceramic plug has a contact ring therein having an interior surface adapted for making electrical contact with said contact plug, and a contact surface, and wherein said metal tube has a lateral opening therein exposing said contact surface for establishing electrical contact to said interior of said housing.

5 16. A pacemaker housing as claimed in claim 15 wherein said contact ring comprises a metal ring attached to said ceramic plug by an attachment technique selected from molding and bonding, and wherein said ceramic plug has an exterior with an opening therein in registration with said lateral opening in said metal tube allowing access to said ring from an exterior of said tube.

10 18. A pacemaker housing as claimed in claim 17 wherein said metal ring has an interior that is free of said ceramic forming a peripheral groove in an interior of said ring allowing access to said ring from said interior of said metal tube.

IN THE DRAWINGS

Please amend each of Figures 1, 2 and 5 as shown on the drawing copies marked in red attached to the Request for Approval of Drawing Changes filed simultaneously herewith.

15 **IN THE ABSTRACT**

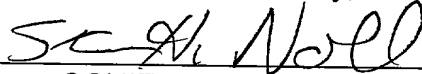
Please add the Abstract on separately numbered page 16 attached hereto.

REMARKS

The present Amendment makes changes in the specification, claims, drawings, and adds an Abstract, to conform the application to the requirements of United States patent practice. The claims submitted herein are considered to be commensurate in scope with the originally filed claims, and therefore the cancellation of claims 1-9 is not considered by the Applicants as a surrender of any of the subject matter encompassed within the original claims, nor are the claims presented herein considered to be narrower than the originally-filed claims.

Early consideration on the merits is respectfully requested.

Submitted by,



(Reg. 28,982)

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Attorneys for Applicants.

ABSTRACT OF THE DISCLOSURE

A pacer housing has a pacemaker housing having a connector arrangement which is adapted to receive a contact plug at the proximal end of a lead, the pacemaker housing having a housing enclosure made of metal and the connector arrangement forming a tubular member with two opposite ends disposed inside of the housing. A first end of the tubular member is open and is welded or bonded to an opening in the wall of the housing. The second end of the tubular member is closed. The tubular member is made of metal that is weldable or bondable to the metal housing. The tubular member is structurally intact along its entire length. A number of interior components, adapted for mechanical and electrical contact with contact surfaces of the contact plug of the lead, are held in an insulating ceramic plug which is located in the interior of the tubular member and is coaxial therewith.



SUBSTITUTE SPECIFICATION

SPECIFICATION

TITLE

"A HOUSING, WITH A TUBULAR CONNECTOR, FOR A HEART STIMULATOR"

5 BACKGROUND OF THE INVENTION

Field of the Invention

The present invention relates to pacemaker housings and more particularly to those parts of the housing intended for connection to the electrode leads.

Description of the Prior Art

Implantable pacers normally have a pacer housing (also called can) containing electronic circuitry and a unit for electric power as well as different electrodes which are connected to the interior parts in the pacer housing and which are to be implanted in or in the vicinity of the heart. The electrodes are connected to the pacer by means of leads. The internal parts of the pacers have to be well protected against the internal environment, especially the body fluids in the body for a long period of time, which places strict requirements on all entries into the interior of the can and especially on the connections of the leads to the housing. At the same time it should be possible to disconnect the pacer from the implanted leads for replacement or servicing of the pacer. The connective parts of the pacer and the leads have largely been standardized so as to encompass a relatively deep female socket comprising a number of contact surfaces whereas the leads are provided with a male part comprising one or several corresponding peripheral, generally circular contact surfaces.

25 At present the connective part of the pacer housing containing the female socket is made of a transparent material, normally epoxy resin, which is molded onto the housing and onto contacts extending outwardly from the housing. The male part of the leads is normally locked by means of set-screws, although other fastening means have been envisaged. The

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positioning and alignment of the different contact surfaces and of the fastening means or metallic threads for the set screws prior to the molding of the connective part is however very complicated and the delay in the manufacturing process incurred by the curing of the epoxy resin is considerable.

It would thus be desirable if the molding procedure could be dispensed with.

It has been discussed that these complexities could be avoided by designing the pacemaker with a socket located inside the metal housing. This kind of socket, sometimes termed "black holes", is not used at present.

United States Patent Nos 4,934,366 and 5,324,111, the teachings of both of which are incorporated herein by reference, describe two interior sockets or black holes for pacemakers. Both designs have a tubular member formed by a number of alternating sections made of metal and insulating ceramic, respectively. An end section of metal can be welded or bonded to an opening in the pacemaker housing by means of a flange. The use of different materials, however, sets high standards in regard of precision and durability of the component parts and as well as on the assembly procedure thereof. This is especially important since the interior sockets must meet very high standards regarding the integrity of the interior of the pacemaker housing during long times of implantation in a demanding environment. The manufacture of these known sockets thus is relatively complicated. The same is true for the device disclosed in United States Patent No. 4,262,982, a ceramic socket combined with a metal flange for welding to a pacemaker housing and with a metallic interior contact pin. This device also has locking means in the form of an inwardly directed, circumferential rib located adjacent the opening of socket. This rib is intended to cooperate with barb-shaped sealing rings on the contact plug on the proximal end of the lead or catheter.

SUMMARY OF THE INVENTION

It is an object of the invention to provide a pacer housing which allows the molding procedure to be avoided and the design of an interior socket to be simplified to a high degree while still meeting the required high standards

5 The above object is achieved in accordance with the principles of the present invention in a pacemaker housing having a connector arrangement which is adapted to receive a contact plug at the proximal end of a lead, the pacemaker housing having a housing enclosure made of metal and the connector arrangement forming a tubular member with two opposite ends
10 disposed inside of the housing. A first end of the tubular member is open and is welded or bonded to an opening in the wall of the housing. The second end of the tubular member is closed. The tubular member is made of metal that is weldable or bondable to the metal housing. The tubular member is structurally intact along its entire length. A number of interior
15 components, adapted for mechanical and electrical contact with contact surfaces of the contact plug of the lead, are held in an insulating ceramic plug which is located in the interior of the tubular member and is coaxial therewith.

DESCRIPTION OF THE DRAWINGS

20 Figure 1 is a side view of a conventional pacer housing having a transparent molded connector part.

 Figure 2 shows a lead with a male connector plug, of the type used with the inventive pacer housing.

25 Figure 3 shows an exploded view of various components of a connective part constructed in accordance with the principles of the present invention.

 Figure 4 is a side sectional view of an assembled connective part constructed in accordance with the principles of the present invention.

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Figure 5 is a side sectional view of a portion of a pacemaker housing constructed in accordance with the principles of the present invention with a connector plug of an electrode lead inserted therein.

5 Figure 6 is a side sectional view of a further embodiment of a connective part constructed in accordance with the principles of the present invention.

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DESCRIPTION OF THE PREFERRED EMBODIMENTS

Fig 1 illustrates a conventional pacemaker housing 1 having a molded, transparent connective part 2. The connective part 2 includes a female socket 3. The inner end of the socket 3 is provided with a longitudinal bore 7 having a relatively small diameter. The bore 7 is provided with a contact surface 4 adjacent to which threads for a set or lock screw are located in a bore 6 oriented orthogonally relative to the female socket. The housing 2 is hermetically sealed in relation to the molded part 2 and the contact between the interior electronics and the contact surface 4 is achieved by means of a feed-through. The feed-through is a ceramic plug, typically made of alumina, into which one or more leads have been soldered. This lead is bonded (e.g. ultrasonically welded) to the electronics and to the contact surface 4. The ceramic plug is soldered or brazed with gold into a sleeve made of titanium. This operation may be done at any time before the assembly of the pacemaker housing 2. The sleeve is welded into an opening in the housing 2 in a sealing manner during the assembly of the pacemaker housing 2, that normally is formed by two halves. Before the connective part is molded onto the housing, these halves are welded together and sealed.

Fig 2 illustrates a lead 15 having a proximal connecting plug 10 and a distal, transvenous, intracardial electrode 16 as well as an attachment element 17 for suturing the proximal end of the lead in the body of the patient. The connecting plug 10 is designed to be received in the socket 3 and the end thereof is provided with a longitudinally projecting contact pin 11 as well as a cylindrical body provided with sealing rings 12, 13, 14 intended to engage and seal against the corresponding inner cylindrical surface of the female socket 3. The shape of the pin 11 corresponds to the shape of the bore 7. When the plug 10 is inserted into the socket 3 the pin 11 engages the contact surface 4 and the set-screw in the bore 6 can be tightened against the pin 11 in order to securely lock the plug 10 in the socket 3. The complexities involved in holding the bores, contact surfaces and threads in

position and keeping them open and free from the molding material during the molding process are evident.

For simplicity, the above prior art device has been illustrated as being unipolar. A bipolar embodiment naturally will be more complex to manufacture. The preferred embodiments of the invention described below will relate to bipolar embodiments.

Figs 3 -5 show a preferred embodiment of the invention having a tubular member 20. For clarity, all reference signs have not been repeated throughout all drawings.

The member has a tube 21 with two open ends 22, 23. One end 22 is to be welded into an opening in the pacemaker housing. The tube 21 is made of the same metal as the pacemaker housing, in this case titanium. The opposite end 23 of the tube 21 is provided with a ceramic plug 26 fitting snugly in the tube and soldered with for instance gold against the inside of the tube 21. One contact ring 27 has been molded or bonded into the ceramic plug.

The ceramic plug is provided with an interior bore corresponding to the shape of the proximal part of the male connector in the same way as the molded prior art female connector described above and thus includes an interior sealing surface 53 for engagement with the sealing rings on the male connector.

The outer side of the Outer end of the contact ring is free from ceramic and extends out past the end of the tube 21, thus forming a contact surface for connection to the interior of the housing.

The inner bore of the ceramic plug is closed by a metal plug 28 having an inner bore at the inner end sized to correspond to the contact pin of the male connector and forming the innermost part of the inner bore of the ceramic plug. The inner bore of the metal plug also comprises an inner, circumferential groove 30. The outer end of the metal plug extends out from the ceramic, past the end of the contact ring 27, thus forming a second

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contact surface. The metal plug may be molded into the ceramic or may be a separate part inserted and bonded into the inner bore of the ceramic plug.

5 The end part 31 of the inside of the contact ring is not covered with the ceramic material. In this way an inner circumferential groove is obtained in the inner bore of the ceramic plug. The bottom of the groove consists of the metal in the contact ring.

10 Thus, when the ceramic plug 26 has been soldered or bonded into place, the second end 23 will be completely sealed by the plug 26 although allowing electrical connection to the interior of the tube via the contact ring 27 and the metal plug 22. It should be noted that several concentric contact rings in a staggered configuration separated by insulating ceramic material could be used. The number of the connections thus would be limited only by the constraints given by the dimensions.

15 The manufacturing steps involved in the above can be carried out in advance as desired so as to achieve a prefabricated tube.

20 The end of the prefabricated tube can be welded to the pacemaker housing and the housing parts can be welded together after the connection of interior leads from the interior electronics to the contact ring and the plug, should this be desired. The remaining parts, i.e. the means achieving the contact between the contact rings and the contact surfaces on the male connector part on the lead and the means locking or fixating the male connector part in the socket, can easily be inserted afterwards. This means for instance that these parts would not interfere with the standard helium-based procedures for testing the housing with connector for leaks or that these parts would not be affected by the leak testing procedure.

25 Fig 3 shows the main components of the tubular member, the tube 21 with the ceramic plug 26, a locking arrangement 40 and two circular spring contacts 50, 51. The spring contacts are similar to the spring contacts used in United States Patent No. 4,934,366.

The locking arrangement 40 is designed in a similar way as the lead locking device disclosed in United States Patent No. 4,262,982, herewith incorporated by reference.

5 The tube 21 preferably is of the same material as the pacer housing, which normally is made of titanium. The ceramic plug may for instance be made of alumina Al_2O_3 , and the contact rings may for instance be made of stainless steel or of titanium.

10 Fig 4 shows the tubular connective member in an assembled state and Fig 5 shows the tubular connective member mounted in a pacer housing 60. The male connector plug 110 is shown inserted into the connective member.

15 The lead locking arrangement 40 has a resilient ring 70 10 mounted in an interior, circumferential groove 71 in an inner sealing surface 54 in a hollow locking cylinder 41 fitting in the open end of the tube 21. The resilient ring is mounted so as to be located directly behind the hindmost sealing ring 116 on the plug 110. The resilient ring has an inner circumferential locking flange 72 biased inwardly into the central bore. When the plug 110 is inserted into the connective member, the sealing rings 112 - 116 thus will pass the flange and the hindmost sealing ring 116 will be held
20 by the flange 72 against a movement outwardly from the connective member 40. Other lead locking means that could be used in this embodiment are for instance disclosed in United States Patent No. 4,934,366, the teachings of which are incorporated herein by reference.

25 Fig 5 shows how the tube has been mounted in a pacer housing 60 and welded to an opening 61 in the housing via flanges located on the outside of the tube ends. Fig 5 also shows a male connector plug 110 inserted in the tubular member. The plug has a contact pin 111, a contact surface 112 and four sealing rings 112, 113, 114, 116. The sealing rings 112 - 114, 116 are in engagement with the interior sealing surfaces 53, 54 and

the spring contacts are in contact pin 111 respectively with the contact surface 118.

The connector means can be achieved in a simple way compared with the prior art molded connector means.

5 As mentioned above, the ceramic part can be soldered into the tube in advance by similar methods as used when obtaining the feed-through in the prior art. The tube then is placed in the opening in one of the pacer housing halves and may supported by a support 62 located in the housing, should this prove desirable. The support in this case is a bracket being a
10 part of the inner module in the pacer housing having an opening that is complementary to the outside of the tube. Conductors 55, 56 are bonded (typically by means of ultrasonic welding) to the connecting parts of the an electronic circuit board 57 and to the parts of the contact ring and the metal plug that are accessible at the end of the tube. The housing halves then are
15 assembled and the two halves and the ends of the tube are welded together by means of a laser beam to form a sealed unit. This unit then is tested for leakage, for instance by means of standard helium-based procedures. It should be noted that no other kinds of work operations than those already used in the prior art are necessary.

20 The pacer then is finished by slipping the resilient spring contacts into the respective interior grooves in the ceramic plug and by inserting and bonding the lead locking means into place in the open end of the tube.

 The new connective part thus is very simple to manufacture and to mount in the pacer housing. The welding and sealing of the housing only
25 includes the additional step of welding the ends of the tube to the edges of the openings in the housing, which is performed in the same operation as the welding of the two housing halves. After the welding operation, no further operations are necessary, except for the simple insertion of spring contact rings and lead-locking mechanism.

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Since the tube after the welding operation in principle forms an integral part of the pacer housing, a high degree of tightness and integrity is obtained. The tube will ensure a high strength and a high durability of the connective part, whilst the ceramic plug will ensure a high degree of tightness in view of the large contact area between ceramic plug and tube that can be used for soldering, i.e. sealing.

One important feature of the invention is the ability to achieve a high capacitance between contact ring and tube. The ring and tube will be separated by the ceramic, which is chosen to be insulating and thus is a dielectricum.

The preferred embodiment naturally has a high capacitance since the contact ring has to extend a long way along the tube. This capacitance of course can be increased if a capacitor is connected in-between the outer tube and the contact ring.

In an alternative embodiment, illustrated in Fig 6, the mid-section of the tube is provided with two relatively small lateral openings 124, 125. The openings 124, 125 are sealed by means of a ceramic plug 126 fitting snugly in the tube and soldered with gold or otherwise bonded against the inside of the tube. Two contact rings 127, 128 have been molded into the ceramic plug.

The ceramic plug is provided with an interior bore corresponding to the shape of the proximal part of the male connector in the same way as the molded prior art female connector described above. The ceramic plug thus includes an interior sealing surface 153 for engagement with sealing rings on the male connector.

The central part 130, 131 of the inside of the contact rings is not covered with the ceramic material. In this way two inner circumferential grooves are obtained in the inner bore of the ceramic plug. The bottom of the grooves consists of the metal in the contact rings. Two openings 132, 133 are also provided in the outer surface of the ceramic plug that may be

made to coincide with the lateral openings 124, 125 in the tube wall. These openings allow access to the contact rings 127, 128 when the ceramic plug has been mounted correctly in the tube 121. Leads for contacting the interior of the housing can be bonded to the parts of the contact rings 127, 128 accessible through the openings 124 125 and 132, 133.

Thus, when the ceramic plug 126 has been soldered or bonded into place, the openings 124, 125 will be completely sealed by the plug 126 although allowing electrical connection between the interior of the tube and the interior of the housing via the contact rings 127, 128.

The inner end 123 of the tube 121 is closed by means of a ceramic plug 170 soldered into the tube. The plug 170 may be made in one piece with the plug 126 or, as illustrated, in a separate piece.

The grooves 130, 131 contain spring contact rings 150, 151 of the same type as the ones described in the preferred embodiment described above.

The locking arrangement 140 is located in the same place and are identical to the locking arrangement described in the above preferred embodiment. The locking arrangement therefore is not described in more detail here.

It should be noted that the size of the openings 124, 125 being necessary to allow the bonding of the leads to the parts of the contact rings accessible through the openings 124, 125 and 131, 132 is small, in relation to the entire circumference and to the length of the tube. The openings thus do not affect the structural integrity of the tube. The contact rings 127, 128 moreover overlap the openings and are bonded thereto by means of the intermediate layer of ceramics, in this way strengthening the area in which the openings are located.

Typical dimensions for a tube intended to house a standard IS-1 male connector are for instance an inner diameter of 5 mm., a wall thickness of 0.3 mm (i.e. the same as the thickness of typical pacemaker housing walls) and

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a diameter of the holes 124, 125 of about 2 mm. A minimum area of about 4 mm² is necessary for the equipment presently used for bonding leads to metallic surfaces. The length of the tube is of course adapted to the specific housing into which it is to be placed, but might typically be about 25 mm.

5 These dimensions of course can be varied as long as the tube remains structurally intact, i.e. as long as the tube has a strength and rigidity that is sufficient to prevent loads, including thermal stresses, on the housing and/or the connector to be transferred as tensile forces to the ceramic parts. Of course, low tensile forces not exceeding the tensile strength of the
10 ceramic could be accepted. Since there are standards regarding the loads a pacer housing and connector should be able to withstand and regarding the overall tightness of the housing, variations of the dimensions only would involve standard stress calculations and dimensioning well within the scope of the man in the art. It should be noted that this also could take the degree
15 of soldering between ceramic plug and tube into account, since this would determine the extent to which tube and ceramic would function as a composite without going outside the ordinary skill of the man skilled in the art.

20 The number of lateral openings of course only is limited by the length of the tube and by the above considerations regarding the structural integrity.

 It should also be noted that the main design features of the above two embodiments could be combined in different ways. One or several of the connections of the above first embodiment thus could be combined with one or several connections according to the above second embodiment. For
25 instance, should it be desired to provide four contact means for a lead with four conductors, two of them could for instance be connected via an end plug designed in accordance with the first embodiment and the other two by means of lateral openings designed in accordance with the second embodiment.

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It should also be noted that the ceramic material in the connector partly or entirely could be replaced by another insulating material, for instance a suitable plastics material.

- 5 Although modifications and changes may be suggested by those skilled in the art, it is the intention of the inventors to embody within the patent warranted hereon all changes and modifications as reasonably and properly come within the scope of their contribution to the art.

1.00280 6E20E960

24.5.2001

09/020229

A HOUSING, WITH A TUBULAR CONNECTOR, FOR A HEART STIMULATOR

Technical field of the invention.

5 The present invention relates to pacemaker housings and more particularly to those parts of the housing intended for connection to the electrode leads.

Background of the invention.

10 Implantable pacemakers normally comprise a pacemaker housing (also called can) containing electronic circuitry and a unit for electric power as well as different electrodes which are connected to the interior parts in the pacemaker housing and which are to be implanted in or in the vicinity of the heart. The electrodes are connected to the pacemaker by means of

15 leads. The internal parts of the pacemakers have to be well protected against the internal environment, especially the body fluids in the body for a long period of time, which places strict requirements on all entries into the interior of the can and especially on the connections of the leads to

20 the housing. At the same time it should be possible to disconnect the pacemaker from the implanted leads for replacement or servicing of the pacemaker. The connective parts of the pacemaker and the leads have largely been standardized so as to encompass a relatively deep female socket comprising a

25 number of contact surfaces whereas the leads are provided with a male part comprising one or several corresponding peripheral, generally circular contact surfaces.

At present the connective part of the pacemaker housing

30 containing the female socket is made of a transparent material, normally of epoxy resin, which is molded onto the housing and onto contacts extending outwardly from the housing. The male part of the leads is normally locked by means of set-screws, although other fastening means have

35 been envisaged. The positioning and alignment of the different contact surfaces and of the fastening means or metallic threads for the set screws prior to the molding of the connective part is however very complicated and the

delay in the manufacturing process incurred by the curing of the epoxy resin is considerable.

It would thus be desirable if the molding procedure could be
5 dispensed with.

It has been discussed that these complexities could be avoided by designing the pacemaker with a socket located inside the metal housing. To our knowledge this kind of sockets,
10 sometimes termed "black holes", are not used at present.

US-A-4,934,366 and US-A-5,324,311, both of which are incorporated by reference, describe two interior sockets or black holes for pacemakers. Both designs comprise a tubular
15 member consisting of a number of alternating sections made of metal respectively of insulating ceramics. An end section of metal can be welded or bonded to an opening in the pacemaker housing by means of a flange. The use of different materials however set high standards in regard of precision and
20 durability of the component parts and as well as on the assembly procedure thereof. This is especially important since the interior sockets must meet very high standards regarding the integrity of the interior of the pacemaker housing during long times of implantation in a demanding
25 environment. The manufacture of these prior art sockets thus is relatively complicated. The same is valid for the device disclosed in US-A-4,262,982, a ceramic socket combined with a metal flange for welding to a pacemaker housing and with a metallic interior contact pin. This device also comprises
30 locking means in the form of an inwardly directed, circumferential rib located adjacent the opening of socket. This rib is intended to cooperate with barb-shaped sealing rings on the contact plug on the proximal end of the lead or catheter.

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Short description of the inventive concept

According to the invention the molding procedure can be avoided and the design of an interior socket can be

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simplified to a high degree whilst still meeting the required high standards by designing a pacemaker housing in accordance with the appended main claim. Preferred embodiments are set forth in the dependent claims.

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Short description of the appended drawings

Fig 1 shows a conventional pacemaker housing with a transparent, molded connective part;

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Fig 2 shows a lead with a male connective part;

Figs 3 - 5 show a preferred embodiment of the connective part in accordance with the present invention;

15

Fig 6 illustrates an alternative embodiment of the invention.

Detailed description of preferred embodiments of the invention.

20

Fig 1 illustrates a conventional pacemaker housing 1 having a molded, transparent connective part 2. The connective part 2 includes a female socket 3. The inner end of the socket 3 is provided with a longitudinal bore 7 having a relatively small diameter. The bore 7 is provided with a contact surface 4 adjacent to which threads 5 for a set or lock screw are located in a bore 6 oriented orthogonally relative to the female socket. The housing is hermetically sealed also in relation to the molded part 2 and the contact between the interior electronics and the contact surface 4 is achieved by means of a feed-through. The feed-through comprises a ceramic plug, typically made of alumina, into which one or more leads have been soldered. This lead is bonded (e.g. ultrasonically welded) to the electronics and to the contact surface 4. The ceramic plug is soldered or brazed by means of gold into a sleeve made of titanium. This operation may be made at any time before the assembly of the

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pacemaker housing. The sleeve is welded into an opening in the housing in a sealing manner during the assembly of the pacemaker housing that normally consists of two halves. Before the connective part is molded onto the housing, these halves are
5 welded together and sealed.

Fig 2 illustrates a lead 15 comprising a proximal connecting plug 10 and a distal, transvenous, intracardial electrode 16 as well as an attachment means 17 for suturing the proximal
10 end of the lead in the body of the patient. The connecting plug 10 is designed to be received in the socket 3 and the end thereof is provided with a longitudinally projecting contact pin 11 as well as a cylindrical body 17 provided with sealing rings 12, 13, 14 intended to engage and seal
15 against the corresponding inner cylindrical surface of the female socket 3. The shape of the pin 11 corresponds to the shape of the bore 7. When the plug 10 is inserted into the socket 3 the pin 11 engages the contact surface 4 and the set-screw in the bore 6 can be tightened against the pin 11
20 in order to securely lock the plug 10 in the socket 3. The complexities involved in holding the bores, contact surfaces and threads in position and keeping them open and free from the molding material during the molding process are evident.

25 For the sake of simplicity, the above prior art device has been illustrated as being unipolar. A bipolar embodiment naturally will be more complex to manufacture. The preferred embodiments of the invention described below will relate to bipolar embodiments.

30 Figs 3 - 5 show a preferred embodiment of the invention comprising a tubular member 20. For the sake of clarity, all reference signs have not been repeated throughout all drawings.

35 The member comprises a tube 21 with two open ends 22, 23. One end 22 is to be welded into an opening in the pacemaker housing. The tube is made of the same metal as the pacemaker

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housing, in this case titanium. The opposite end 23 of the tube is provided with a ceramic plug 26 fitting snugly in the tube and soldered with for instance gold against the inside of the tube. One contact ring 27 has been molded or
5 bonded into the ceramic plug.

The ceramic plug is provided with an interior bore corresponding to the shape of the proximal part of the male connector in the same way as the molded prior art female
10 connector described above and thus includes an interior sealing surface 53 for engagement with the sealing rings on the male connector.

The outer side of the outer end of the contact ring is free
15 from ceramic and extends out past the end of the tube 21, thus forming a contact surface for connection to the interior of the housing.

The inner bore of the ceramic plug is closed by a metal plug
20 28 having an inner bore at the inner end sized to correspond to the contact pin of the male connector and forming the innermost part of the inner bore of the ceramic plug. The inner bore of the metal plug also comprises an inner, circumferential groove 30. The outer end of the metal plug
25 extends out from the ceramic, past the end of the contact ring 27, thus forming a second contact surface. The metal plug may be molded into the ceramic or may be a separate part inserted and bonded into the inner bore of the ceramic plug.

30 The end part 31 of the inside of the contact ring is not covered with the ceramic material. In this way an inner circumferential groove is obtained in the inner bore of the ceramic plug. The bottom of the groove consists of the metal
35 in the contact ring.

Thus, when the ceramic plug 26 has been soldered or bonded into place, the second end 23 will be completely sealed by

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the plug 26 although allowing electrical connection to the interior of the tube via the contact ring 27 and the metal plug 28. It should be noted that several concentric contact rings in a staggered configuration separated by insulating ceramic material could be used. The number of the connections thus only would be limited by the constraints given by the dimensions.

The manufacturing steps involved in the above can be carried out in advance as desired so as to achieve a prefabricated tube.

The end of the prefabricated tube can be welded to the pacemaker housing and the housing parts can be welded together after the connection of interior leads from the interior electronics to the contact ring and the plug, should this be desired. The remaining parts, i. e. the means achieving the contact between the contact rings and the contact surfaces on the male connector part on the lead and the means locking or fixating the male connector part in the socket, can easily be inserted afterwards. This means for instance that these parts would not interfere with the standard helium-based procedures for testing the housing with connector for leaks or that these parts would not be affected by the leak testing procedure.

Fig 3 shows the main component parts of the tubular member, the tube 21 with the ceramic plug 26, a fixation part 40 and two circular spring contacts 50, 51. The spring contacts are similar to the spring contacts used in US-A-4,934,366.

The fixation part 40 is designed in a similar way as the lead locking device disclosed in US-A-4,262,982, herewith incorporated by reference,

The tube 21 preferably is of the same material as the pacemaker housing, which normally is made of titanium. The ceramic plug may for instance be made of alumina, Al_2O_3 , and the

contact rings may for instance be made of stainless steel or of titanium.

Fig 4 shows the tubular connective member in an assembled state and Fig 5 shows the tubular connective member mounted in a pacemaker housing 60. The male connector plug 110 is shown inserted into the connective member.

The lead locking means 40 comprises a resilient ring 70 mounted in an interior, circumferential groove 71 in an inner sealing surface 54 in a hollow locking cylinder 41 fitting in the open end of the tube 21. The resilient ring is mounted so as to be located directly behind the hindmost sealing ring 116 on the plug 110. The resilient ring comprises an inner circumferential locking flange 72 biased inwardly into the central bore. When the plug 110 is inserted into the connective member, the sealing rings 112 - 116 thus will pass the flange and the hindmost sealing ring 116 will be held by the flange 72 against a movement outwardly from the connective member 40. Other lead locking means that could be used in this embodiment are for instance disclosed in US-A-4,934,366, which document thus is incorporated by reference.

Fig 5 shows how the tube has been mounted in a pacemaker housing 60 and welded to an opening 61 in the housing via flanges located on the outside of the tube ends. Fig 5 also shows a male connector plug 110 inserted in the tubular member. The plug has a contact pin 111, a contact surface 118 and four sealing rings 112, 113, 114, 116. The sealing rings 112 - 114, 116 are in engagement with the interior sealing surfaces 53, 54 and the spring contacts are in contact pin 111 respectively with the contact surface 118.

The connector means can be achieved in a simple way compared with the prior art molded connector means.

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As mentioned above, the ceramic part can be soldered into the tube in advance by similar methods as used when obtaining the feed-through in the prior art. The tube then is placed in the opening in one of the pacer housing halves and may supported by a support 62 located in the housing, should this prove desirable. The support in this case is a bracket being a part of the inner module in the pacer housing having an opening that is complementary to the outside of the tube. Conductors 55, 56 are bonded (typically by means of ultrasonic welding) to the connecting parts of the electronic boards 57 and to the parts of the contact ring and the metal plug that are accessible at the end of the tube. The housing halves then are assembled and the two halves and the ends of the tube are welded together by means of a laser beam to form a sealed unit. This unit then is tested for leakage, for instance by means of standard helium-based procedures. It should be noted that no other kinds of work operations than those already used in the prior art are necessary.

The pacer then is finished by slipping the resilient spring contacts into the respective interior grooves in the ceramic plug and by inserting and bonding the lead locking means into place in the open end of the tube.

The new connective part thus is very simple to manufacture and to mount in the pacer housing. The welding and sealing of the housing only includes the additional step of welding the ends of the tube to the edges of the openings in the housing, which is performed in the same operation as the welding of the two housing halves. After the welding operation, no further operations are necessary, except for the simple insertion of spring contact rings and lead-locking mechanism.

Since the tube after the welding operation in principle forms an integral part of the pacer housing, a high degree of tightness and integrity is obtained. The tube will ensure

a high strength and a high durability of the connective part, whilst the ceramic plug will ensure a high degree of tightness in view of the large contact area between ceramic plug and tube that can be used for soldering, i.e. sealing.

5

One important feature of the invention is the possibility of achieving a high capacitance between contact ring and tube. Ring and tube will be separated by the ceramic, which is chosen to be insulating and thus is a dielectricum.

10

The preferred embodiment naturally has a high capacitance since the contact ring has to extend a long way along the tube. This capacitance of course can be increased if a capacitor is connected in-between the outer tube and the contact ring.

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In an alternative embodiment, illustrated in Fig 6, the mid-section of the tube is provided with two relatively small lateral openings 124, 125. The openings 124, 125 are sealed by means of a ceramic plug 126 fitting snugly in the tube and soldered with gold or otherwise bonded against the inside of the tube. Two contact rings 127, 128 have been molded into the ceramic plug.

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The ceramic plug is provided with an interior bore corresponding to the shape of the proximal part of the male connector in the same way as the molded prior art female connector described above. The ceramic plug thus includes an interior sealing surface 153 for engagement with sealing rings on the male connector.

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The central part 130, 131 of the inside of the contact rings is not covered with the ceramic material. In this way two inner circumferential grooves are obtained in the inner bore of the ceramic plug. The bottom of the grooves consists of the metal in the contact rings. Two openings 132, 133 are also provided in the outer surface of the ceramic plug that may be made to coincide with the lateral openings 124, 125

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in the tube wall. These openings give access to the contact rings 127, 128 when the ceramic plug has been mounted correctly in the tube 121. Leads for contacting the interior of the housing can be bonded to the parts of the contact rings 127, 128 accessible through the openings 124 125 and 132, 133.

Thus, when the ceramic plug 126 has been soldered or bonded into place, the openings 124, 125 will be completely sealed by the plug 126 although allowing electrical connection between the interior of the tube and the interior of the housing via the contact rings 127, 128.

The inner end 123 of the tube 121 is closed by means of a ceramic plug 170 soldered into the tube. The plug 170 may be made in one piece with the plug 126 or, as illustrated, in a separate piece.

The grooves 130, 131 contain spring contact rings 150, 151 of the same type as the ones described in the preferred embodiment described above.

The locking means 140 are located in the same place and are identical to the locking means described in the above preferred embodiment. The locking means therefore are not described in more detail here.

It should be noted that the size of the openings 124, 125 being necessary to allow the bonding of the leads to the parts of the contact rings accessible through the openings 124, 125 and 131, 132 is small, seen in relation to the entire circumference and to the length of the tube. The openings thus do not affect the structural integrity of the tube. The contact rings 127, 128 moreover overlap the openings and are bonded thereto by means of the intermediate layer of ceramics, in this way strengthening the area in which said openings are located.

Typical dimensions for a tube intended to house a standard IS-1 male connector are for instance an inner diameter of 5 mm, a wall thickness of 0.3 mm (i. e. the same as the thickness of typical pacer housing walls) and a diameter of the holes 124, 125 of about 2 mm. A minimum area of about 4 mm² is necessary for the equipment presently used for bonding leads to metallic surfaces. The length of the tube is of course adapted to the specific housing into which it is to be placed, but might typically be about 25 mm.

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These dimensions of course can be varied as long as the tube remains structurally intact, i. e. as long as the tube has a strength and rigidity that is sufficient to prevent loads, including thermal stresses, on the housing and/or the connector to be transferred as tensile forces to the ceramic parts. Of course, low tensile forces not exceeding the tensile strength of the ceramic could be accepted. Since there are standards regarding the loads a pacer housing and connector should be able to withstand and regarding the overall tightness of the housing, variations of the dimensions only would involve standard stress calculations and dimensioning well within the scope of the man in the art. It should be noted that this also could take the degree of soldering between ceramic plug and tube into account, since this would determine the extent to which tube and ceramic would function as a composite without going outside the ordinary skill of the man skilled in the art.

The number of lateral openings of course only is limited by the length of the tube and by the above considerations regarding the structural integrity.

It should also be noted that the main design features of the above two embodiments could be combined in different ways. One or several of the connections of the above first embodiment thus could be combined with one or several connections according to the above second embodiment. For instance, should it be desired to provide four contact means

for a lead with four conductors, two of them could for instance be connected via an end plug designed in accordance with the first embodiment and the other two by means of lateral openings designed in accordance with the second
5 embodiment.

It should also be noted that the ceramic material in the connector partly or entirely could be replaced by another insulating material, for instance a suitable plastics
10 material.

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CLAIMS

1. Pacer housing (60) comprising a connector means adapted to receive a contact plug (110) on the proximal end of a lead (15) with an electrode located on the distal end of said lead, said housing being made of metal, said connector means comprising a tubular member having two ends and being located inside said housing, a first end (22, 122) of said tubular member being welded or bonded to an opening in a wall of said housing, the second end (23, 123) of said tubular member being closed, characterized in that said tubular member comprises a tube (21, 121) made of a metal being weldable or bondable to said metal housing, said tube being structurally intact along its entire length, all interior means (27, 127, 28, 128, 50, 150, 51, 151) in said tube for contacting the contact surfaces (111, 118) on said plug being located within the enclosure formed by said tube, said tube further containing at least one insulating plug (26, 126) being coaxial with said tube and holding said interior means for contacting said contact surfaces on said plug.
2. Pacer housing according to claim 1, characterized in that said second end (23, 123) is closed by means of said insulating plug (26, 126) fitting into said metal tube, said plug being made of a ceramic material and being soldered or bonded to said tube.
3. Pacer housing according to claim 2, characterized in that at least one contact means for contact with the interior of the housing is located on the outside of a metallic tubular sleeve (27) embedded in said ceramic plug (26), said sleeve extending out from said ceramic plug so as to provide an exterior contact surface for contacting the interior of said housing, the inside of the opposite end of said sleeve being exposed so as to provide an inner contact surface (31) for contacting said contact plug.

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4. Pacer housing according to any one of claims 2 or 3, characterized in that a metallic plug (28) is embedded in said ceramic plug, the outer end of said plug (28) extending out from said ceramic plug (26) so as to provide an exterior contact surface for contacting the interior of said housing.

5. Pacer housing according to claim 4, characterized in that a part of the opposite, inner end of said metallic plug (28) is provided with an inner bore providing an interior contact surface (30) for contacting said contact plug.

6. Pacer housing according to claim 1, characterized in that said metal tube (121) is provided with one or several lateral contact openings (124, 125), contact ring surfaces (127, 128) for establishing the contact to the interior of said housing being located in said opening(s) (124, 125), said contact surfaces being electrically connected to said means (50, 51) for contacting said contact surfaces (111, 118) on said plug (110).

7. Pacer housing according to claim 6, characterized in that said opening(s) (124, 125) are closed by means of said at least one insulating ceramic plug (126) fitting into said metal tube, said ceramic plug being soldered or bonded to said tube, said plug holding said contact means (127, 128) for contacting the interior of said housing.

8. Pacer housing according to claim 7, characterized in that said contact means comprise metal rings (127, 128) that are molded or bonded into the ceramic plug (126), the outside of said ceramic plug (126) being provided with openings (132, 133) corresponding to said lateral openings (124, 125) in said tube, thus giving access to said rings (127, 128) from the outside of said tube.

9. Pacer housing according to claim 7 or 8, characterized in that the central part of the inside of said metal rings (127, 128) is free from said ceramic, thus providing a

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Fig. 1

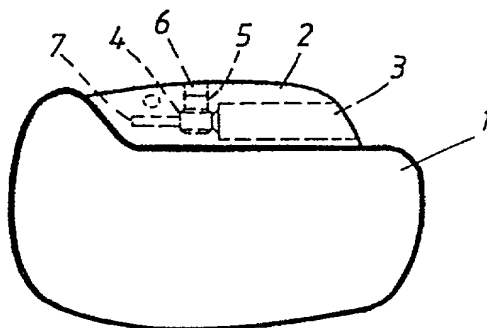


Fig. 2

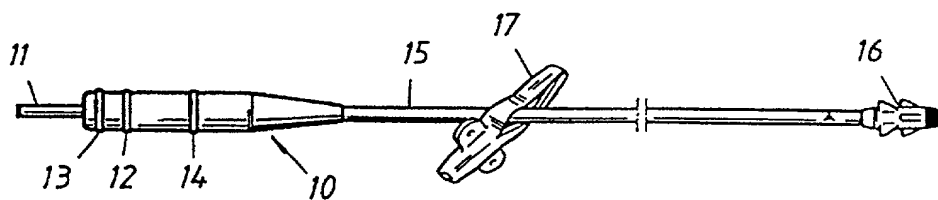
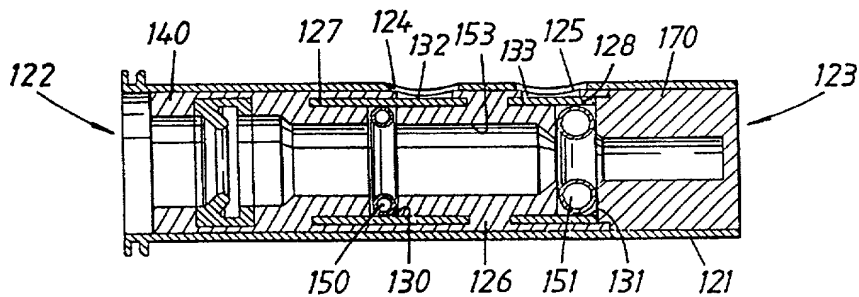


Fig. 6



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Fig. 3

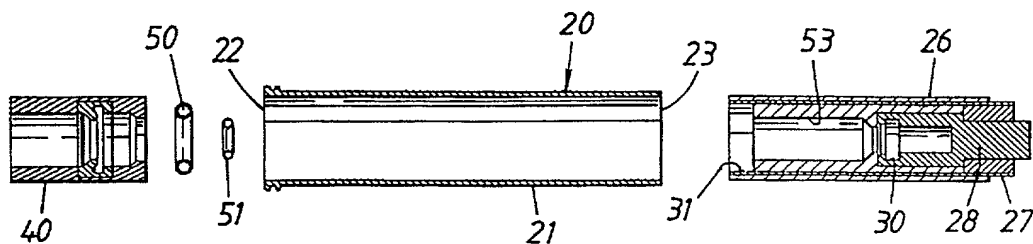


Fig. 4

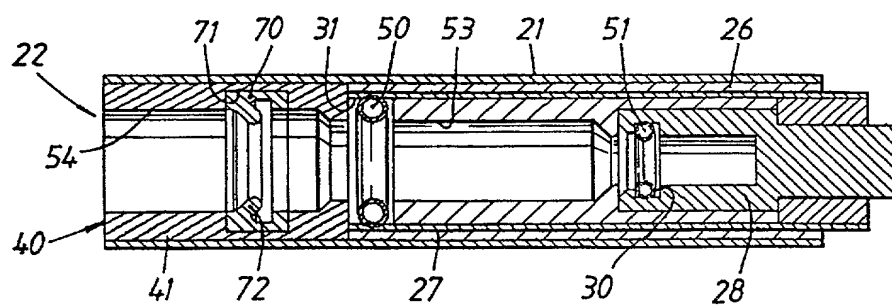
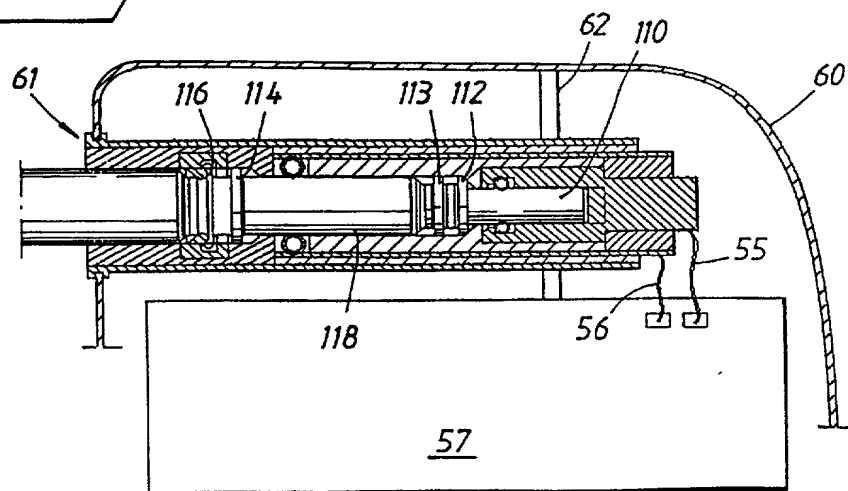


Fig. 5





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[A HOUSING, WITH A TUBULAR CONNECTOR, FOR A HEART STIMULATOR

Technical field of the invention.]

SPECIFICATION

TITLE

**"A HOUSING, WITH A TUBULAR CONNECTOR,
FOR A HEART STIMULATOR"**

BACKGROUND OF THE INVENTION

Field of the Invention

The present invention relates to pacemaker housings and more particularly to those parts of the housing intended for connection to the electrode leads.

[Background of the invention.]

Description of the Prior Art

Implantable pacers normally [comprise] have a pacer housing (also called can) containing electronic circuitry and a unit for electric power as well as different electrodes which are connected to the interior parts in the pacer housing and which are to be implanted in or in the vicinity of the heart. The electrodes are connected to the pacer by means of leads. The internal parts of the pacers have to be well protected against the internal environment, especially the body fluids in the body for a long period of time, which places strict requirements on all entries into the interior of the can and especially on the connections of the leads to the housing. At the same time it should be possible to disconnect the pacer from the implanted leads for replacement or servicing of the pacer. The connective parts of the pacer and the leads have largely been standardized so as to encompass a relatively deep female socket comprising a number of contact surfaces whereas the leads are provided with a male part comprising one or several corresponding peripheral, generally circular contact surfaces.

At present the connective part of the pacer housing containing the female socket is made of a transparent material, normally [of] epoxy resin, which is molded onto the housing and onto contacts extending outwardly from the housing. The male part of the leads is normally locked by means of set-screws, although other fastening means have been envisaged. The positioning and alignment of the different contact surfaces and of the fastening means or metallic threads for the set screws prior to the molding of the connective part is however very complicated and the delay in the manufacturing process incurred by the curing of the epoxy resin is considerable.

It would thus be desirable if the molding procedure could be dispensed with.

It has been discussed that these complexities could be avoided by designing the pacer with a socket located inside the metal housing. [To our knowledge this] This kind of [sockets] socket, sometimes termed "black holes", [are] is not used at present.

[US-A-4,934,366 and US-A--5,324,311] United States Patent Nos 4,934,366 and 5,324,111, the teachings of both of which are incorporated herein by reference, describe two interior sockets or black holes for pacers. Both designs [comprise] have a tubular member [consisting of] formed by a number of alternating sections made of metal [respectively of] and insulating [ceramics] ceramic, respectively. An end section of metal can be welded or bonded to an opening in the pacer housing by means of a flange. The use of different materials, however, sets [set] high standards in regard of precision and durability of the component parts and as well as on the assembly procedure thereof. This is especially important since the interior sockets must meet very high standards regarding the integrity of the interior of the pacer housing during long times of implantation in a demanding environment. The manufacture of these [prior art] known sockets thus is relatively complicated. The same is [valid] true for the device disclosed in

[US-A-4,262,982] United States Patent No. 4,262,982, a ceramic socket combined with a metal flange for welding to a pacer housing and with a metallic interior contact pin. This device also [comprises] has locking means in the form of an inwardly directed, circumferential rib located adjacent the opening of socket. This rib is intended to cooperate with barb-shaped sealing rings on the contact plug on the proximal end of the lead or catheter.

[Short description of the inventive concept]

SUMMARY OF THE INVENTION

[According to] It is an object of the invention to provide a pacer housing which allows the molding procedure [can] to be avoided and the design of an interior socket [can] to be simplified to a high degree [whilst] while still meeting the required high standards [by designing a pacer housing in accordance with the appended main claim. Preferred embodiments are set forth in the dependent claims].

The above object is achieved in accordance with the principles of the present invention in a pacemaker housing having a connector arrangement which is adapted to receive a contact plug at the proximal end of a lead, the pacemaker housing having a housing enclosure made of metal and the connector arrangement forming a tubular member with two opposite ends disposed inside of the housing. A first end of the tubular member is open and is welded or bonded to an opening in the wall of the housing. The second end of the tubular member is closed. The tubular member is made of metal that is weldable or bondable to the metal housing. The tubular member is structurally intact along its entire length. A number of interior components, adapted for mechanical and electrical contact with contact surfaces of the contact plug of the lead, are held in an insulating ceramic plug which is located in the interior of the tubular member and is coaxial therewith.

[Short description of the appended drawings

Fig 1 shows a conventional pacer housing with a transparent, molded connective part;

Fig 2 shows a lead with a male connective part;

5 Figs 3 - 5 show a preferred embodiment of the connective part in accordance with the present invention;

Fig 6 illustrates an alternative embodiment of the invention.

Detailed description of preferred embodiments of the invention.]

DESCRIPTION OF THE DRAWINGS

10 Figure 1 is a side view of a conventional pacer housing having a transparent molded connector part.

Figure 2 shows a lead with a male connector plug, of the type used with the inventive pacer housing.

15 Figure 3 shows an exploded view of various components of a connective part constructed in accordance with the principles of the present invention.

Figure 4 is a side sectional view of an assembled connective part constructed in accordance with the principles of the present invention.

20 Figure 5 is a side sectional view of a portion of a pacer housing constructed in accordance with the principles of the present invention with a connector plug of an electrode lead inserted therein.

Figure 6 is a side sectional view of a further embodiment of a connective part constructed in accordance with the principles of the present invention.

DESCRIPTION OF THE PREFERRED EMBODIMENTS

Fig 1 illustrates a conventional pacemaker housing 1 having a molded, transparent connective part 2. The connective part 2 includes a female socket 3. The inner end of the socket 3 is provided with a longitudinal bore 7 having a relatively small diameter. The bore 7 is provided with a contact surface 4 adjacent to which threads for a set or lock screw are located in a bore 6 oriented orthogonally relative to the female socket. The housing 2 is hermetically sealed [also] in relation to the molded part 2 and the contact between the interior electronics and the contact surface 4 is achieved by means of a feed-through. The feed-through [comprises] is a ceramic plug, typically made of alumina, into which one or more leads have been soldered. This lead is bonded (e.g. ultrasonically welded) to the electronics and to the contact surface 4. The ceramic plug is soldered or brazed [by means of] with gold into a sleeve made of titanium. This operation may be [made] done at any time before the assembly of the pacemaker housing 2. The sleeve is welded into an opening in the housing 2 in a sealing manner during the assembly of the pacemaker housing 2, that normally [consists of] is formed by two halves. Before the connective part is molded onto the housing, these halves are welded together and sealed.

Fig 2 illustrates a lead 15 [comprising] having a proximal connecting plug 10 and a distal, transvenous, intracardial electrode 16 as well as an attachment [means] element 17 for suturing the proximal end of the lead in the body of the patient. The connecting plug 10 is designed to be received in the socket 3 and the end thereof is provided with a longitudinally projecting contact pin 11 as well as a cylindrical body [17] provided with sealing rings 12, 13, 14 intended to engage and seal against the corresponding inner cylindrical surface of the female socket 3. The shape of the pin 11 corresponds to the shape of the bore 7. When the plug 10 is inserted into the socket 3 the pin 11 engages the contact surface 4 and the set-screw in the bore 6 can be tightened against the pin 11 in order to securely lock the

plug 10 in the socket 3. The complexities involved in holding the bores, contact surfaces and threads in position and keeping them open and free from the molding material during the molding process are evident.

For [the sake of] simplicity, the above prior art device has been
5 illustrated as being unipolar. A bipolar embodiment naturally will be more complex to manufacture. The preferred embodiments of the invention described below will relate to bipolar embodiments.

Figs 3 -5 show a preferred embodiment of the invention [comprising]
10 having a tubular member 20. For [the sake of] clarity, all reference signs have not been repeated throughout all drawings.

The member [comprises] has a tube 21 with two open ends 22, 23.
One end 22 is to be welded into an opening in the pacer housing. The tube
15 21 is made of the same metal as the pacer housing, in this case titanium. The opposite end 23 of the tube 21 is provided with a ceramic plug 26 fitting snugly in the tube and soldered with for instance gold against the inside of
the tube 21. One contact ring 27 has been molded or bonded into the ceramic plug.

The ceramic plug is provided with an interior bore corresponding to
the shape of the proximal part of the male connector in the same way as the
20 molded prior art female connector described above and thus includes an interior sealing surface 53 for engagement with the sealing rings on the male connector.

The outer side of the Outer end of the contact ring is free 15 from
ceramic and extends out past the end of the tube 21, thus forming a contact
25 surface for connection to the interior of the housing.

The inner bore of the ceramic plug is closed by a metal plug 20 28
having an inner bore at the inner end sized to correspond to the contact pin
of the male connector and forming the innermost part of the inner bore of the
ceramic plug. The inner bore of the metal plug also comprises an inner,
30 circumferential groove 30. The outer end of the metal plug extends out from

the ceramic, past the end of the contact ring 27, thus forming a second contact surface. The metal plug may be molded into the ceramic or may be a separate part inserted and bonded into the inner bore of the ceramic plug.

5 The end part 31 of the inside of the contact ring is not covered with the ceramic material. In this way an inner circumferential groove is obtained in the inner bore of the ceramic plug. The bottom of the groove consists of the metal in the contact ring.

10 Thus, when the ceramic plug 26 has been soldered or bonded into place, the second end 23 will be completely sealed by the plug 26 although allowing electrical connection to the interior of the tube via the contact ring 27 and the metal plug 22. It should be noted that several concentric contact rings in a staggered configuration separated by insulating ceramic material could be used. The number of the connections thus [only] would be limited only by the constraints given by the dimensions.

15 The manufacturing steps involved in the above can be carried out in advance as desired so as to achieve a prefabricated tube.

20 The end of the prefabricated tube can be welded to the pacemaker housing and the housing parts can be welded together after the connection of interior leads from the interior electronics to the contact ring and the plug, should this be desired. The remaining parts, i.e. the means achieving the contact between the contact rings and the contact surfaces on the male connector part on the lead and the means locking or fixating the male connector part in the socket, can easily be inserted afterwards. This means for instance that these parts would not interfere with the standard helium-based
25 procedures for testing the housing with connector for leaks or that these parts would not be affected by the leak testing procedure.

Fig 3 shows the main [component parts] components of the tubular member, the tube 21 with the ceramic plug 26, a [fixation part] locking arrangement 40 and two circular spring contacts 50, 51. The spring contacts

are similar to the spring contacts used in [US-A-4,934,366] United States Patent No. 4,934,366.

5 The [fixation part] locking arrangement 40 is designed in a similar way as the lead locking device disclosed in [US-A-4,262,982] United States Patent No. 4,262,982, herewith incorporated by reference[.].

The tube 21 preferably is of the same material as the pacemaker housing, which normally is made of titanium. The ceramic plug may for instance be made of alumina Al_2O_3 , and the contact rings may for instance be made of stainless steel or of titanium.

10 Fig 4 shows the tubular connective member in an assembled state and Fig 5 shows the tubular connective member mounted in a pacemaker housing 60. The male connector plug 110 is shown inserted into the connective member.

15 The lead locking [means] arrangement 40 [comprises] has a resilient ring 70 10 mounted in an interior, circumferential groove 71 in an inner sealing surface 54 in a hollow locking cylinder 41 fitting in the open end of the tube 21. The resilient ring is mounted so as to be located directly behind the hindmost sealing ring 116 on the plug 110. The resilient ring [comprises] has an inner circumferential locking flange 72 biased inwardly into the central bore. When the plug 110 is inserted into the connective member, the sealing rings 112 - 116 thus will pass the flange and the hindmost sealing ring 116 will be held by the flange 72 against a movement outwardly from the connective member 40. Other lead locking means that could be used in this embodiment are for instance disclosed in [US-A-4,934,366] United States
20 Patent No. 4,934,366, [which document thus is] the teachings of which are
25 incorporated herein by reference.

30 Fig 5 shows how the tube has been mounted in a pacemaker housing 60 and welded to an opening 61 in the housing via flanges located on the outside of the tube ends. Fig 5 also shows a male connector plug 110 inserted in the tubular member. The plug has a contact pin 111, a contact

surface 112 and four sealing rings 112, 113, 114, 116. The sealing rings 112 - 114, 116 are in engagement with the interior sealing surfaces 53, 54 and the spring contacts are in contact pin 111 respectively with the contact surface 118.

5 The connector means can be achieved in a simple way compared with the prior art molded connector means.

As mentioned above, the ceramic part can be soldered into the tube in advance by similar methods as used when obtaining the feed-through in the prior art. The tube then is placed in the opening in one of the pacer housing halves and may supported by a support 62 located in the housing, shou1d this prove desirable. The support in this case is a bracket being a part of the inner module in the pacer housing having an opening that is complementary to the outside of the tube. Conductors 55, 56 are bonded (typically by means of ultrasonic welding) to the connecting parts of the an 10 electronic [boards] circuit board 57 and to the parts of the contact ring and the metal plug that are accessible at the end of the tube. The housing halves then are assembled and the two halves and the ends of the tube are welded together by means of a laser beam to form a sealed unit. This unit then is tested for leakage, for instance by means of standard helium-based 15 procedures. It should be noted that no other kinds of work operations than those already used in the prior art are necessary.

20 The pacer then is finished by s1ipping the resilient spring contacts into the respective interior grooves in the ceramic plug and by inserting and bonding the lead locking means into place in the open end of the tube.

25 The new connective part thus is very simple to manufacture and to mount in the pacer housing. The welding and sealing of the housing only includes the additional step of welding the ends of the tube to the edges of the openings in the housing, which is performed in the same operation as the welding of the two housing halves. After the welding operation, no further

operations are necessary, except for the simple insertion of spring contact rings and lead-locking mechanism.

5 Since the tube after the welding operation in principle forms an integral part of the pacemaker housing, a high degree of tightness and integrity is obtained. The tube will ensure a high strength and a high durability of the connective part, whilst the ceramic plug will ensure a high degree of tightness in view of the large contact area between ceramic plug and tube that can be used for soldering, i.e. sealing.

10 One important feature of the invention is the [possibility of achieving] ability to achieve a high capacitance between contact ring and tube. [Ring] The ring and tube will be separated by the ceramic, which is chosen to be insulating and thus is a dielectricum.

15 The preferred embodiment naturally has a high capacitance since the contact ring has to extend a long way along the tube. This capacitance of course can be increased if a capacitor is connected in-between the outer tube and the contact ring.

20 In an alternative embodiment, illustrated in Fig 6, the mid-section of the tube is provided with two relatively small lateral openings 124, 125. The openings 124, 125 are sealed by means of a ceramic plug 126 fitting snugly in the tube and soldered with gold or otherwise bonded against the inside of the tube. Two contact rings 127, 128 have been molded into the ceramic plug.

25 The ceramic plug is provided with an interior bore corresponding to the shape of the proximal part of the male connector in the same way as the molded prior art female connector described above. The ceramic plug thus includes an interior sealing surface 153 for engagement with sealing rings on the male connector.

30 The central part 130, 131 of the inside of the contact rings is not covered with the ceramic material. In this way two inner circumferential grooves are obtained in the inner bore of the ceramic plug. The bottom of

the grooves consists of the metal in the contact rings. Two openings 132, 133 are also provided in the outer surface of the ceramic plug that may be made to coincide with the lateral openings 124, 125 in the tube wall. These openings [give] allow access to the contact rings 127, 128 when the ceramic plug has been mounted correctly in the tube 121. Leads for contacting the interior of the housing can be bonded to the parts of the contact rings 127, 128 accessible through the openings 124 125 and 132, 133.

Thus, when the ceramic plug 126 has been soldered or bonded into place, the openings 124, 125 will be completely sealed by the plug 126 although allowing electrical connection between the interior of the tube and the interior of the housing via the contact rings 127, 128.

The inner end 123 of the tube 121 is closed by means of a ceramic plug 170 soldered into the tube. The plug 170 may be made in one piece with the plug 126 or, as illustrated, in a separate piece.

The grooves 130, 131 contain spring contact rings 150, 151 of the same type as the ones described in the preferred embodiment described above.

The locking [means] arrangement 140 [are] is located in the same place and are identical to the locking [means] arrangement described in the above preferred embodiment. The locking [means] arrangement therefore [are] is not described in more detail here.

It should be noted that the size of the openings 124, 125 being necessary to allow the bonding of the leads to the parts of the contact rings accessible through the openings 124, 125 and 131, 132 is small, [seen] in relation to the entire circumference and to the length of the tube. The openings thus do not affect the structural integrity of the tube. The contact rings 127, 128 moreover overlap the openings and are bonded thereto by means of the intermediate layer of ceramics, in this way strengthening the area in which [said] the openings are located.

Typical dimensions for a tube intended to house a standard IS-1 male connector are for instance an inner diameter of 5 mm., a wall thickness of 0.3 mm (i.e. the same as the thickness of typical pacer housing walls) and a diameter of the holes 124, 125 of about 2 mm. A minimum area of about 4 mm² is necessary for the equipment presently used for bonding leads to metallic surfaces. The length of the tube is of course adapted to the specific housing into which it is to be placed, but might typically be about 25 mm.

These dimensions of course can be varied as long as the tube remains structurally intact, i.e. as long as the tube has a strength and rigidity that is sufficient to prevent loads, including thermal stresses, on the housing and/or the connector to be transferred as tensile forces to the ceramic parts. Of course, low tensile forces not exceeding the tensile strength of the ceramic could be accepted. Since there are standards regarding the loads a pacer housing and connector should be able to withstand and regarding the overall tightness of the housing, variations of the dimensions only would involve standard stress calculations and dimensioning well within the scope of the man in the art. It should be noted that this also could take the degree of soldering between ceramic plug and tube into account, since this would determine the extent to which tube and ceramic would function as a composite without going outside the ordinary skill of the man skilled in the art.

The number of lateral openings of course only is limited by the length of the tube and by the above considerations regarding the structural integrity.

It should also be noted that the main design features of the above two embodiments could be combined in different ways. One or several of the connections of the above first embodiment thus could be combined with one or several connections according to the above second embodiment. For instance, should it be desired to provide four contact means for a lead with four conductors, two of them could for instance be connected via an end plug designed in accordance with the first embodiment and the other two by

5

Although modifications and changes may be suggested by those skilled in the art, it is the intention of the inventors to embody within the patent warranted hereon all changes and modifications as reasonably and properly come within the scope of their contribution to the art.

Fig. 1

(PRIOR ART)

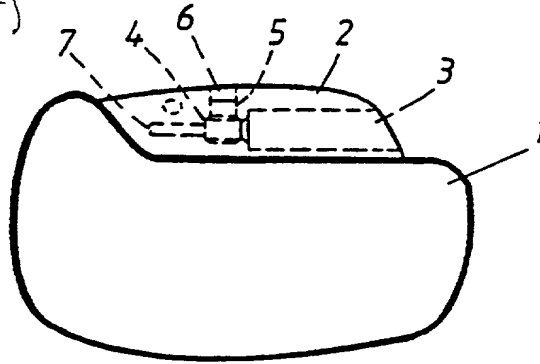


Fig. 2

(PRIOR ART)

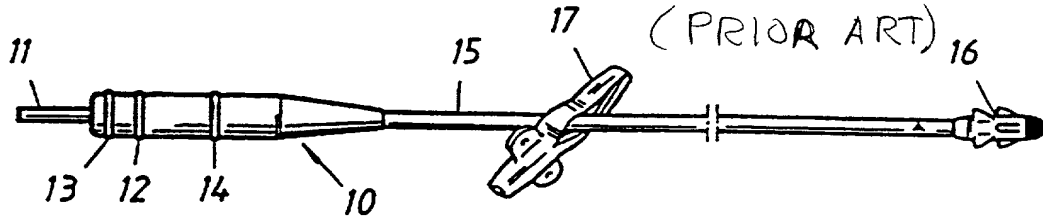


Fig. 6

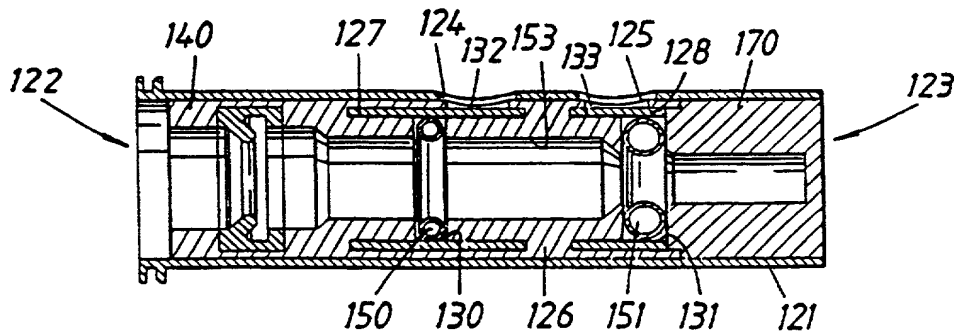


Fig. 3

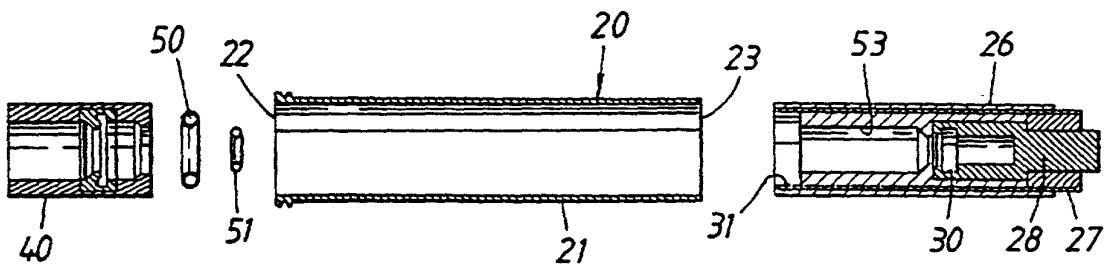


Fig. 4

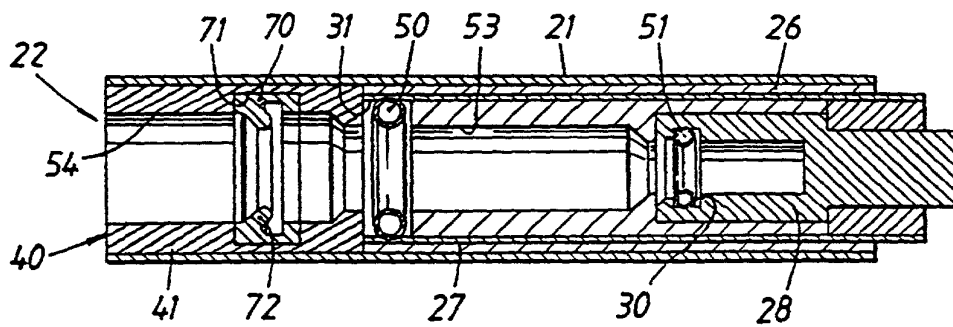
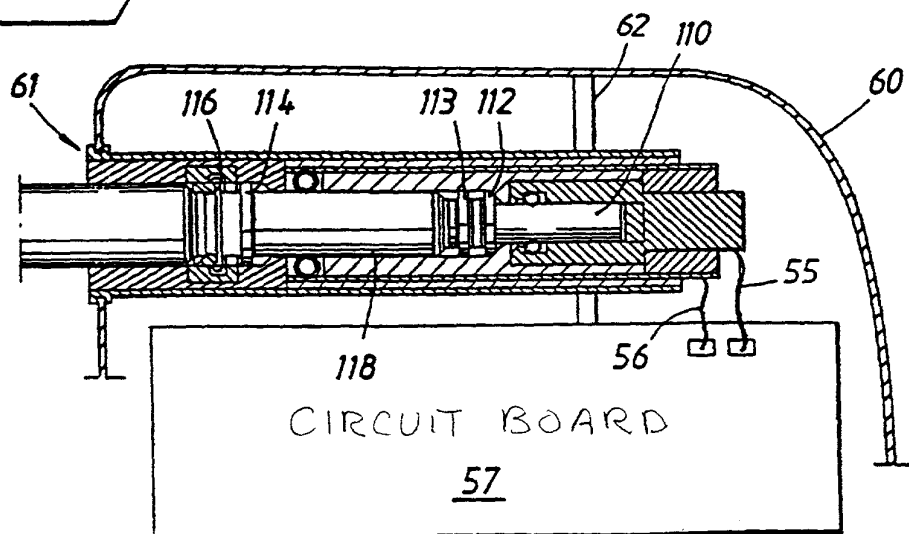


Fig. 5



COMBINED DECLARATION FOR PATENT APPLICATION AND POWER OF ATTORNEYATTORNEY'S
DOCKET NUMBER
P01,0178

(Includes Reference to PCT International Applications)

As a below named inventor, I hereby declare that:

My residence, post office address and citizenship are as stated below next to my name,
I believe I am the original, first and sole inventor (if only one name is listed below) or an original, first and joint
inventor (if plural names are listed below) of the subject matter which is claimed and for which a patent is
sought on the invention entitled:

"A HOUSING, WITH A TUBULAR CONNECTOR, FOR A HEART STIMULATOR"

the specification of which (check only one item below):

- ☐ is attached hereto.
- ☒ was filed as United States application
Serial No. 09/830,239
on April 24, 2001
and was amended
on April 24, 2001 (if applicable).
- ☐ was filed as PCT international application
Number _____
on _____
and was amended under PCT Article 19
on _____ (if applicable).

I hereby state that I have reviewed and understand the content of the above-identified specification, including
the claims, as amended by any amendment referred to above.

I acknowledge the duty to disclose information which is material to the examination of this application in
accordance with Title 37, Code of Federal Regulations, §1.56(a).

I hereby claim foreign priority benefits under Title 35, United States Code, §119 of any foreign application(s) for
patent or inventor's certificate or of any PCT international application(s) designating at least one country other
than the United States of America listed below and have also identified below any foreign application(s) for
patent or inventor's certificate or any PCT international application(s) designating at least one country other
than the United States of America filed by me on the same subject matter having a filing date before that of the
application(s) of which priority is claimed:

PRIOR FOREIGN/PCT APPLICATION(S) AND ANY PRIORITY CLAIMS UNDER 35 U.S.C. 119:

COUNTRY (if PCT Indicate "PCT")	APPLICATION NUMBER	DATE OF FILING (day, month, year)	PRIORITY CLAIMED UNDER 35 USC 119
Sweden	9803693-2	07/19/99	<input checked="" type="checkbox"/> YES <input type="checkbox"/> NO
			<input type="checkbox"/> YES <input type="checkbox"/> NO
			<input type="checkbox"/> YES <input type="checkbox"/> NO
			<input type="checkbox"/> YES <input type="checkbox"/> NO
			<input type="checkbox"/> YES <input type="checkbox"/> NO

Combined Declaration For Patent Application and Power of Attorney (Continued)
(Includes Reference to PCT International Applications)ATTORNEY'S DOCKET NO.
P01,0178

I hereby claim the benefit under Title 35, United States Code, §120 of any United States application(s) or PCT International application(s) designating the United States of America that is/are listed below and, insofar as the subject matter of each of the claims of this application is not disclosed in the prior application(s) in the manner provided by the first paragraph of Title 35, United States Code, §112, I acknowledge the duty to disclose material information as defined in Title 37, Code of Federal Regulations, §1.56(a) which occurred between the filing date of the prior application(s) and the national or PCT International filing date of this application:

PRIOR U.S. APPLICATIONS OR PCT INTERNATIONAL APPLICATIONS DESIGNATING THE U.S. FOR BENEFIT UNDER 35 U.S.C. 120:

U.S. APPLICATIONS		STATUS (Check one)		
U.S. APPLICATION NUMBER	U.S. FILING DATE	PATENTED	PENDING	ABANDONED
PCT APPLICATIONS DESIGNATING THE U.S.				
PCT APPLICATION NO	PCT FILING DATE	U.S. SERIAL NUMBERS ASSIGNED (If any)		

POWER OF ATTORNEY: As a named inventor, I hereby appoint the following attorney(s) and/or agent(s) to prosecute this application and transact all business in the Patent and Trademark Office connected herewith.

And I hereby appoint all Attorneys identified by the United States Patent & Trademark Office Customer Number 26574, who are all members of the firm of Schiff, Hardin & Waite.

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I hereby declare that all statements made herein of my own knowledge are true and that all statements made on information and belief are believed to be true; and further that these statements were made with the knowledge that willful false statements and the like so made are punishable by fine or imprisonment, or both, under section 1001 of Title 18 of the United States Code, and that such willful false statements may jeopardize the validity of the application or any patent issuing thereon.

SIGNATURE OF INVENTOR 201

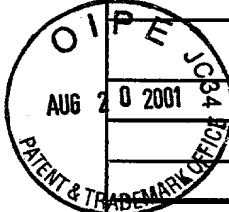
SIGNATURE OF INVENTOR 202

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Aug 15 2001